

1st Journal review

Construction of nonlinear optical microscopy for clinical application

2015/06/17 M2 Atsuta

Nonlinear optical microscopy

In diagnosis, the invasive sampling of physical biopsy takes risks of trauma, infection, hematoma, and hemorrhage

⇒ **Nonlinear optical microscopy**

It is non-invasive and non-contact ,
so physical biopsy diagnosis is NOT needed
on measurement using nonlinear optical
microscopy. (SHG microscopy etc..)



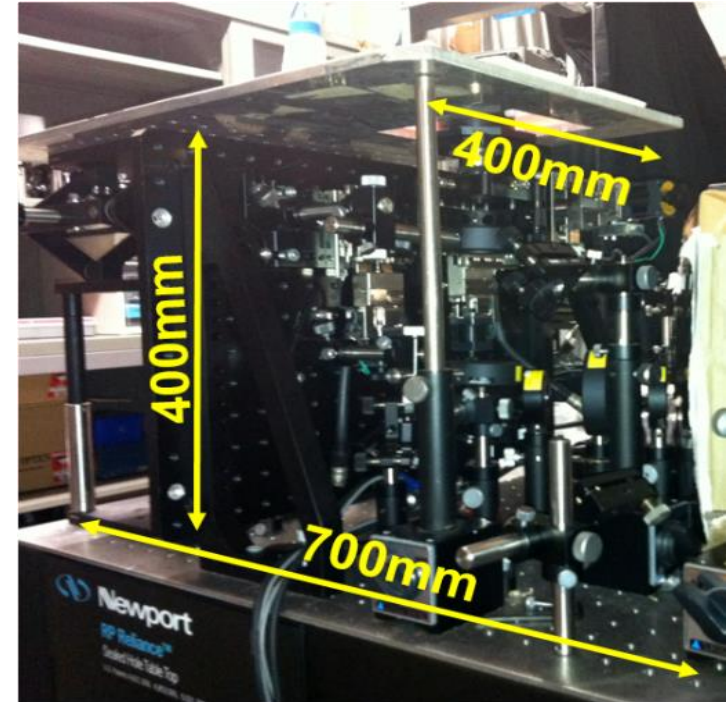
<http://www.momohime-medical.com/>

Nonlinear optical microscopy

For clinical application...

Traditional laboratory microscopes are large scale, inflexible, and free-space beam delivery.

So they are limited its applications.



Optical microscopes need flexible fiber-optical probe

① C. Bechtela, et al. “Large field of view MEMS-based confocal laser scanning microscope for fluorescence imaging” *Optik*.**125**,876 (2013)

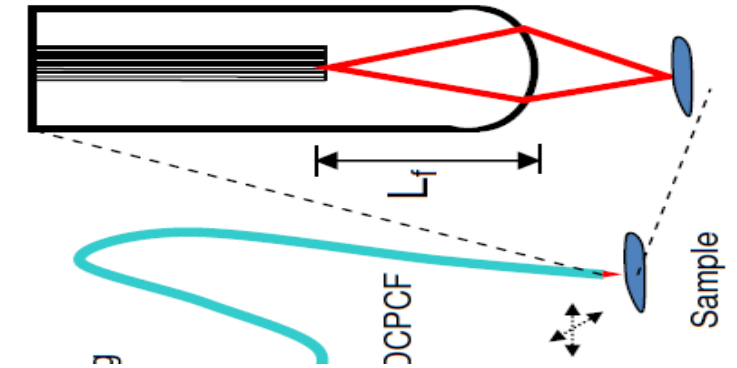
② S. Tang, et al. “Design and implementation of fiber-based multiphoton endoscopy with microelectromechanical systems scanning” *Journal of Biomedical Optics*.**14**, 034005 (2009)

(Fibroblast)

③ B. A. Danowski “Fibroblast contractility and actin organization are stimulated by microtubule inhibitors” *Journal of Cell Science* .**93**, 255 (1990)

① “Large field of view MEMS-based confocal laser scanning microscope for fluorescence imaging”

Introduction Fluorescence confocal laser scanning microscopy F-LSM is now a widely used and powerful imaging technique in fundamental biological and medical research.



Recently...

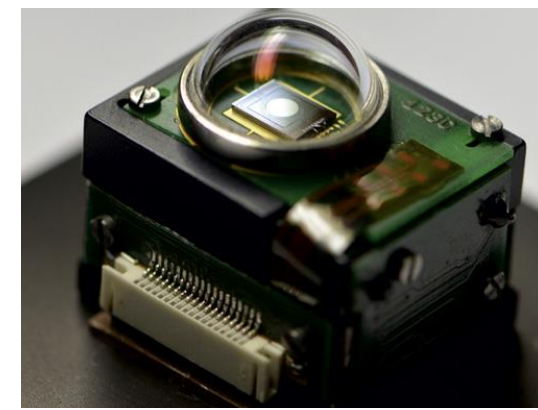
Fibre scan microscopy :

○ **thin probe system** \Rightarrow locally imaging for cell etc...

× **restricted field of view** \Rightarrow unsuitable for skin imaging

space saving, moderately prized system with a large field of view
Using MEMS mirror

the MEMS mirror



$f_{\text{slow}} = 200 \text{ Hz}$, $f_{\text{fast}} = 1.336 \text{ kHz}$

The mirror deflect $\pm 5[\text{deg}]$ $D = 2 \text{ mm}$

twice the total mirror scan angle of 2φ , and the smallest resolvable spot size given by

$$\Delta\varphi = k \lambda \frac{1}{D_{\text{eff}}}$$

Here, k : denoting the aperture shape factor

D_{eff} : effective mirror diameter

The number N_{θ} of resolvable spots for the scanner is given by the ratio of the total optical scan angle θ

$$N_{\theta} = \frac{\theta D_{\text{eff}}}{k \lambda}$$

Here, $\lambda = 520 \text{ nm}$

$$N_{\theta} \approx 990$$

the MEMS mirror

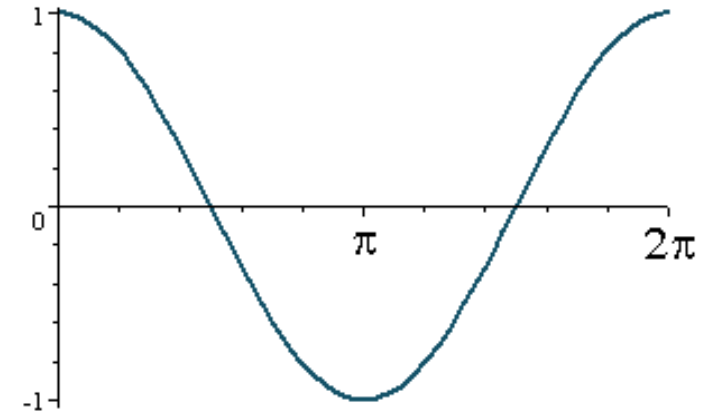
$f_{\text{slow}} = 200 \text{ Hz}$, $f_{\text{fast}} = 1.336 \text{ kHz}$

The mirror deflect $\pm 5[\text{deg}]$ $D = 2 \text{ mm}$

MEMS mirror scan the spot very fast...

So, pixel dwell time has a great impact on the number of photons available for detection.

$$t = \frac{1}{\pi f_{\text{fast}} N_{\theta}}$$



π : the period of one line scan

If, number of photons unavailable for detection,
(As resonant frequency f_{fast} can't change.)

We must change to large number of pixel or high peak power to increase photons.

Field of view

Spot diameter and the Rayleigh range

$$\omega_0 = 0.5k \lambda_{ex} f/\# = 0.49 \mu m$$

$$Z_R = \frac{\pi}{\lambda_{ex}} (\omega_0)^2 = 1.54 \mu m$$

It wants to expand the beam system to 7mm for aperture diameter.

As $M = 7$, Field of view is

$$d_{im} = 2 f \tan\left(2 \frac{\phi}{M}\right) = 500 \mu m$$

Here, ϕ represents the scanning angle of 5°

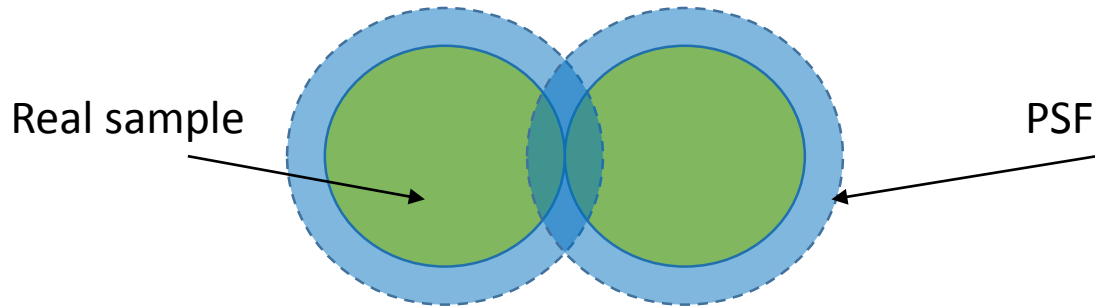
Optical design

The strehl ratio

It represents the smallness of aberration
0.8 is the diffraction limit

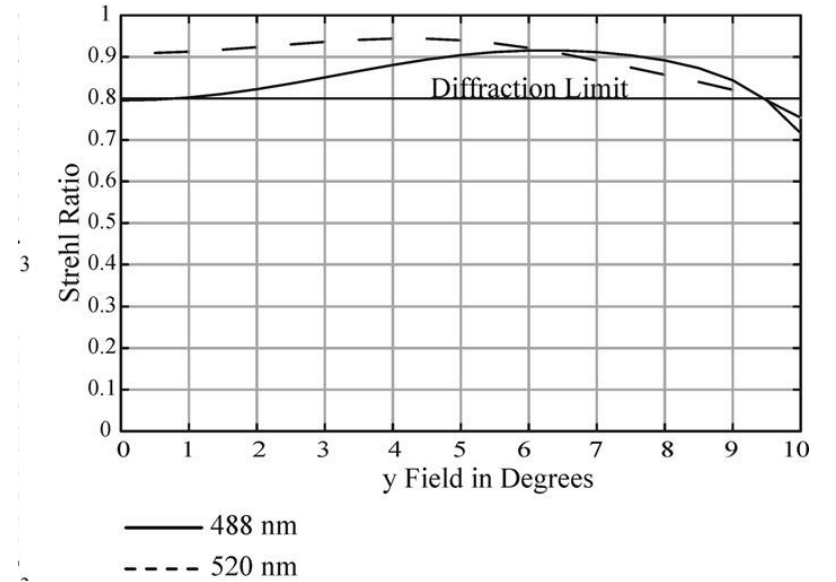
Point Spread Function (PSF)

(Image) = (light spot) + (PSF)

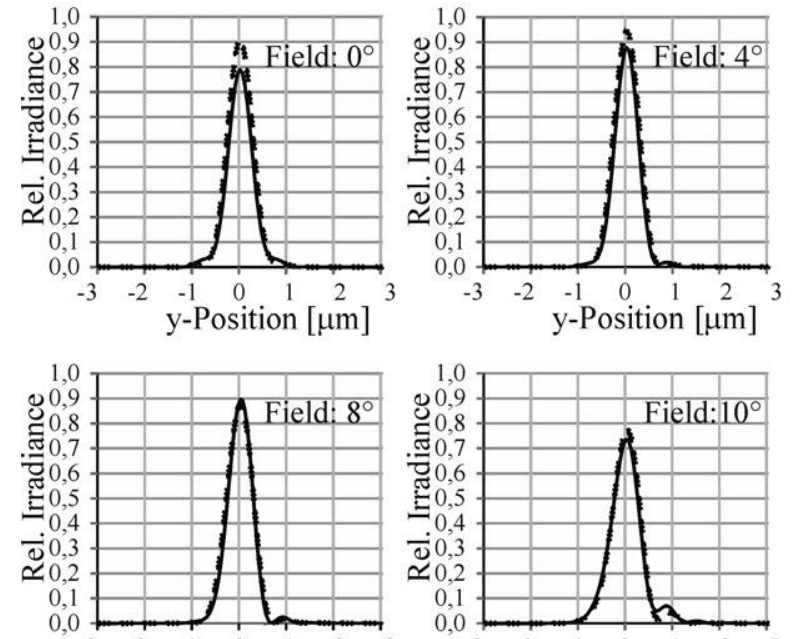


the maximum angle of 10°
the spot size is around $1.2\mu\text{m}$.
This can identify until $6\mu\text{m}$.

b) Strehl Ratio



a) Huygens PSF



Wave aberration from OPD(optical path Difference) in tangential and sagittal direction

Coma aberration occurs between the scan lens
and MEMS mirror

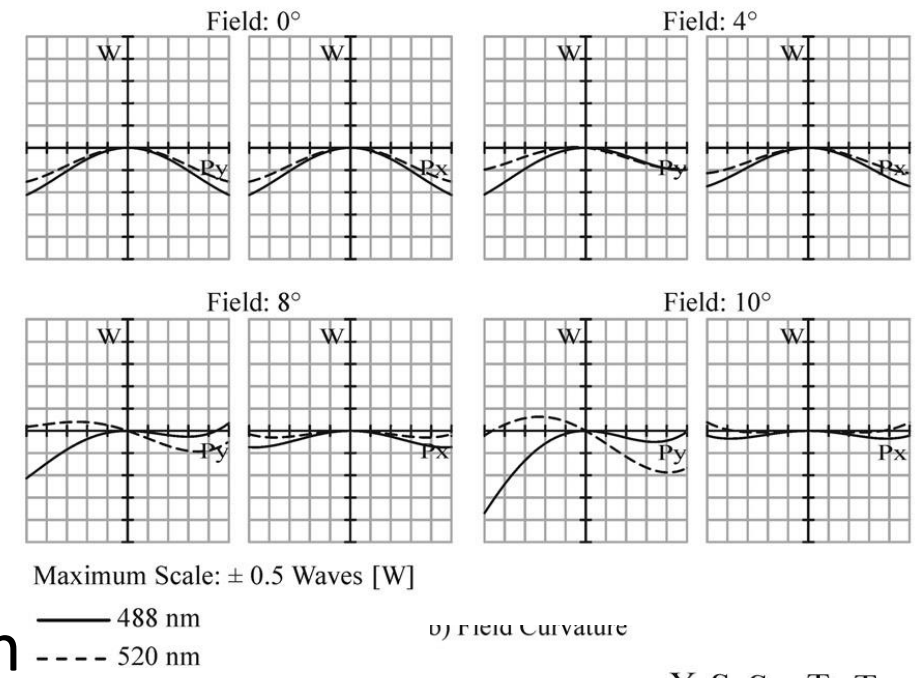
Field curvature

Field curvature in tangential and sagittal direction
coma aberration > spherical aberration.

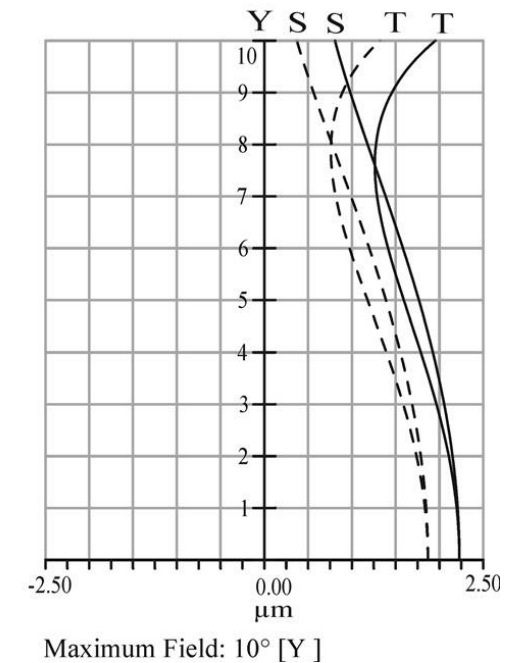
And another characteristic of the system important to look
at is the field curvature

In total these aberrations restrict the maximum scanning
angle to $\pm 10^\circ$. \Rightarrow this design is expected to application
of cell imaging.

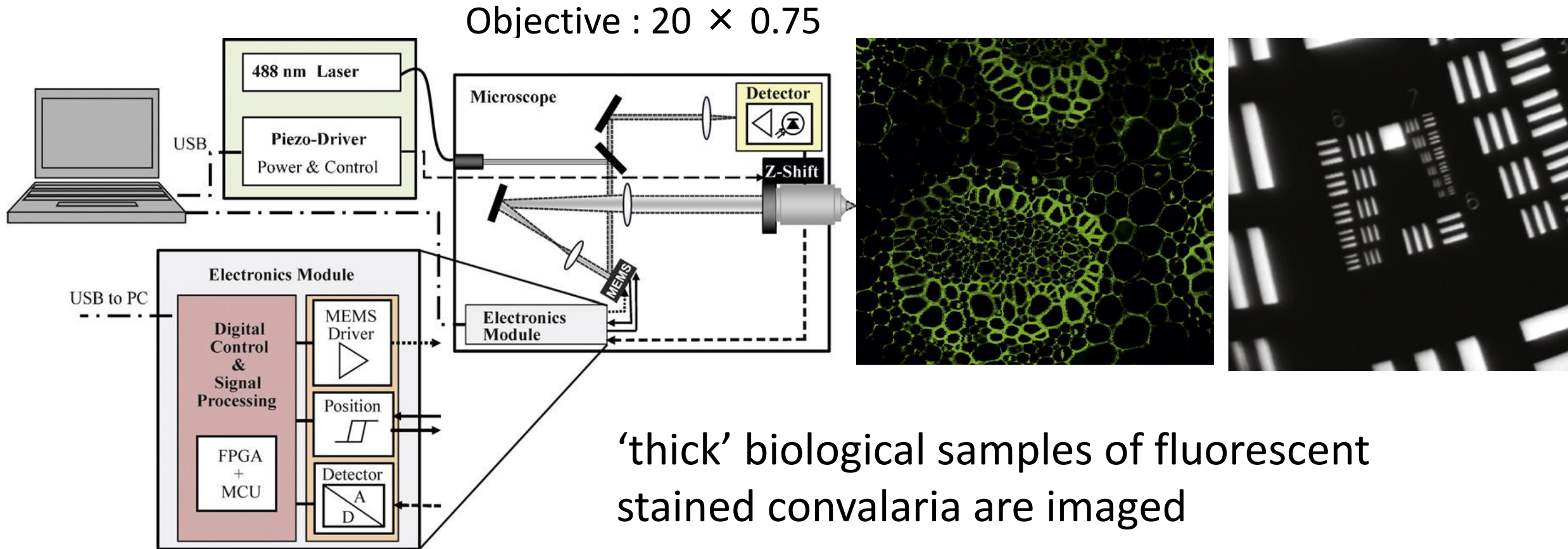
a) Optical Path Difference



b) Field Curvature



Setup and results



‘thick’ biological samples of fluorescent stained convalaria are imaged

In TC, group 7 has 228 line pairs/mm, corresponding to a line width of $2.2\mu\text{m}$.

summary

Confocal fluorescence laser scanning microscopes are well established and widely used in biological and medical research.

First measurements have shown a lateral and axial resolution of $2.2\mu\text{m}$ and $3\mu\text{m}$, respectively with a field of view of $500\mu\text{m} \times 500\mu\text{m}$.

② ”Design and implementation of fiber-based multiphoton endoscopy with microelectromechanical systems scanning”

Introduction

Delivering femtosecond pulses through fibers and designing miniature scanning probes are two challenges in MPM endoscopy.

These problems were solved by DCPCF(Double-cladding photonic crystal fibers) and MEMS mirror.

- ① Comparing SMF, hollow-core PBF, and DCPCF
- ② Three configurations of probe design are discussed, and their advantages and disadvantages are compared.

Setup:

MEMS mirror

Gimbal-less

Mirror diameter 2mm

Al coat (reflectance 80%)

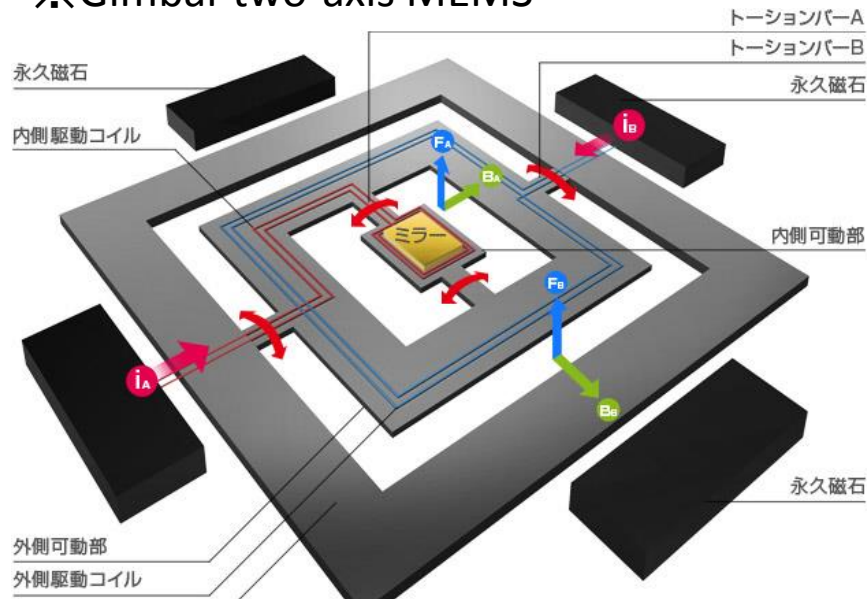
The light source,

Ti: S laser (790nm, bandwidth 10nm,
pulse width 170fs)

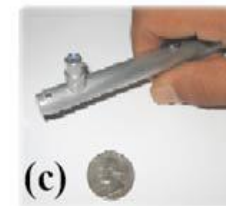
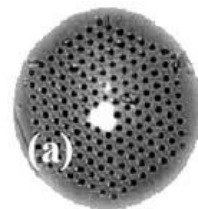
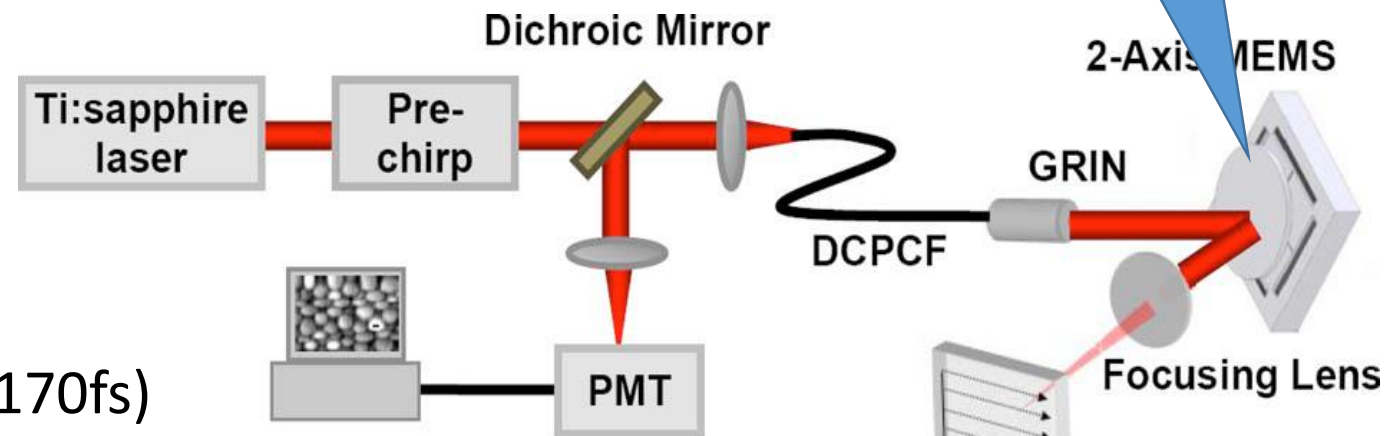
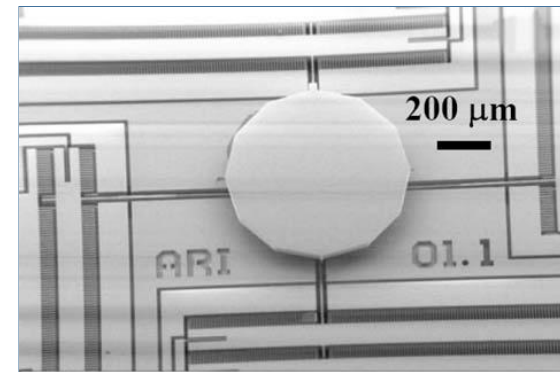
Objective (5 × , NA = 0.1)

Coupling efficiency of 30%

✳Gimbal-two-axis MEMS



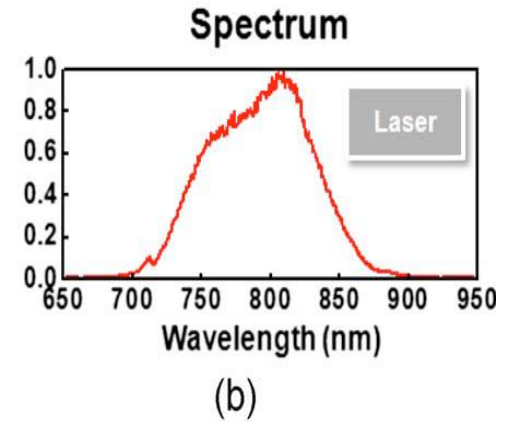
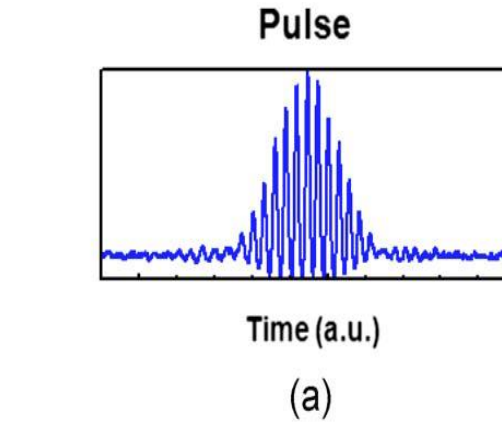
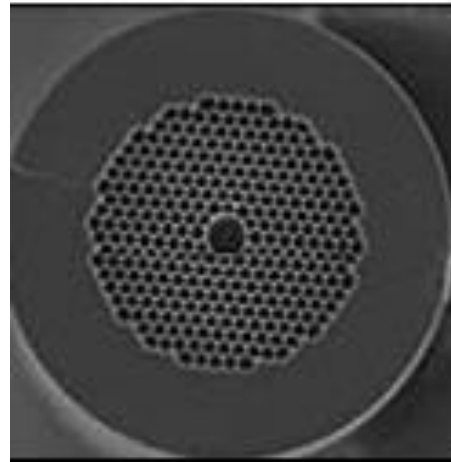
A gimbal-less two-axis MEMS



Fiber delivery

(c)(d)SMF

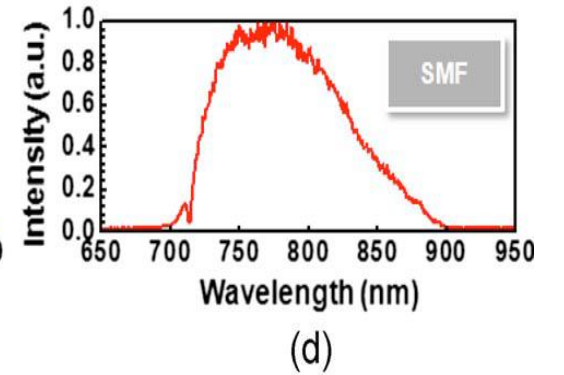
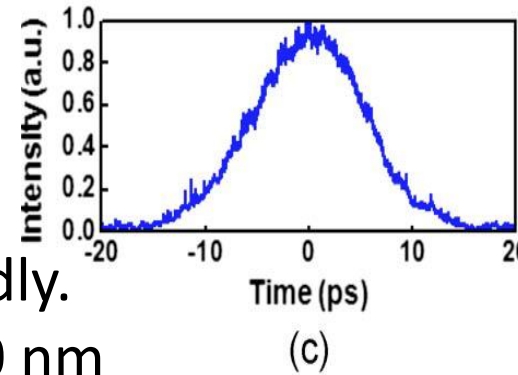
Signal attenuation is negligible
Laser bandwidth increase



(e)(f)Hollow-core PBF

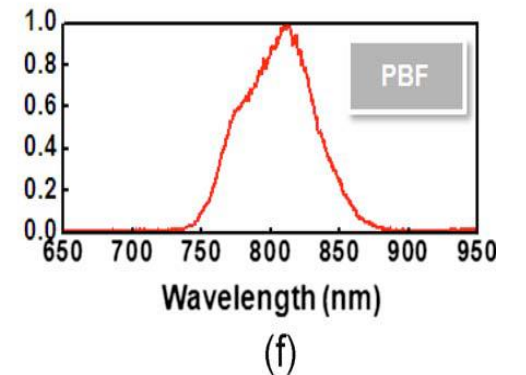
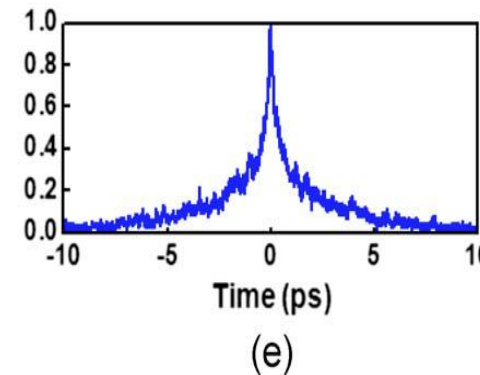
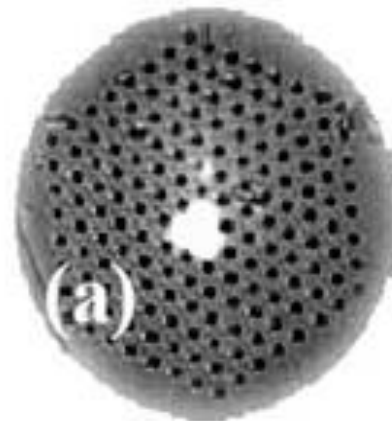
~20 times lower dispersion than SMF

Inside low-loss window, attenuation is low
but outside the window, attenuation increases rapidly.
(window: 90 nm around a center wavelength of 800 nm)



⇒DCPCF

Signal attenuation is negligible
A good collection efficiency with
core and the inner clad



Design:

Design 1 the simplest case

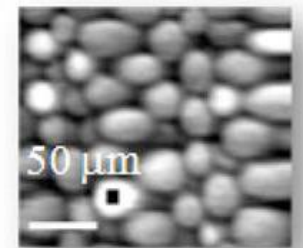
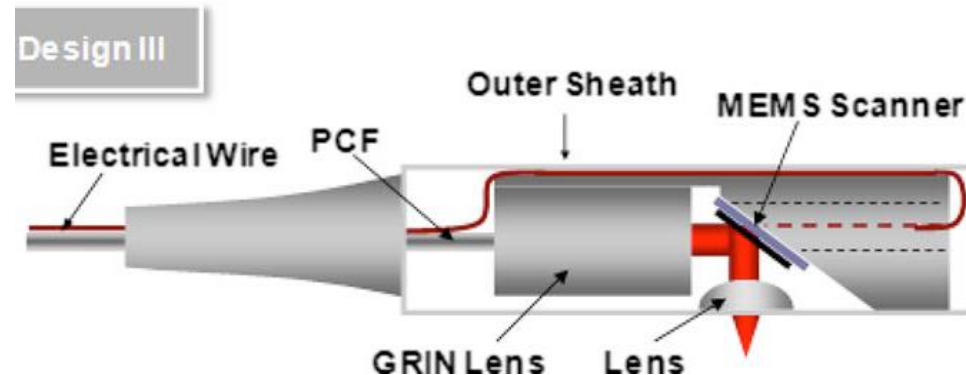
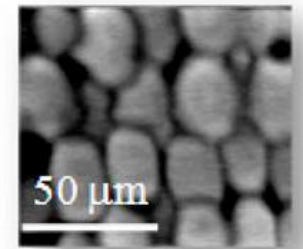
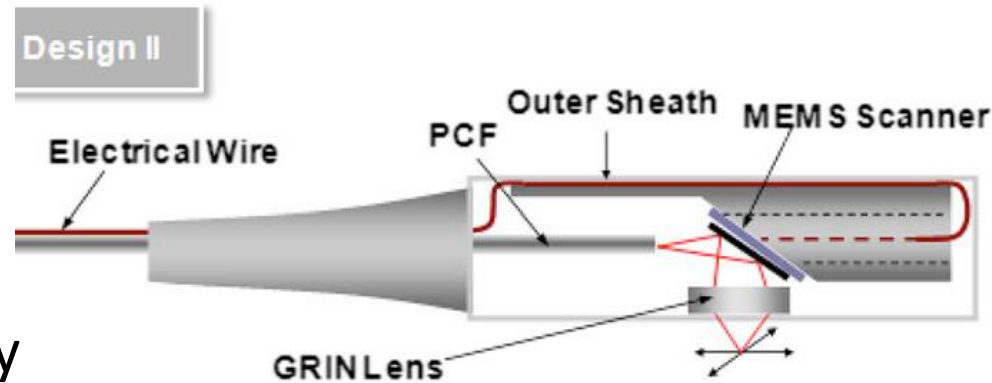
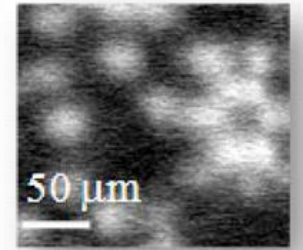
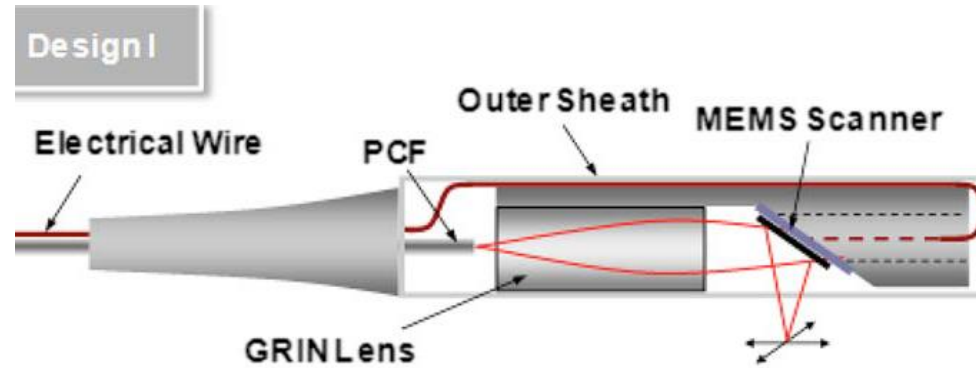
- easy alignment and packaging as well as size efficiency
- × long WD : poor resolution at the focal point.

Design 2

- short WD
- × beam are restricted ⇒ lack of flexibility

Design 3

- provide a collimated beam ⇒ good flexibility



Result

The Fluorescence image

128 * 128 pixels

Frequency, 64Hz and 0.25Hz
(multiphoton fluorescence
is low signal)

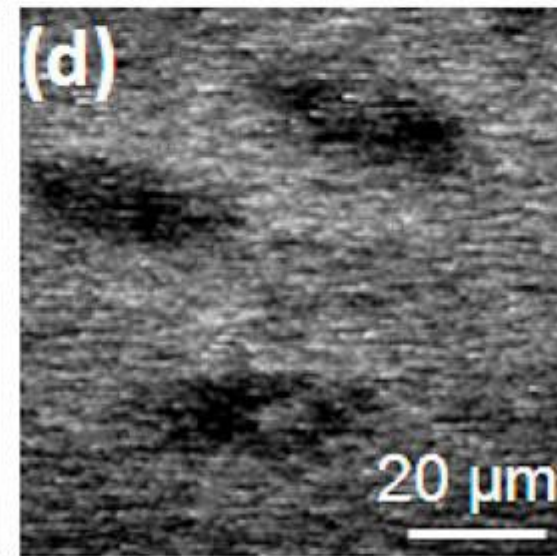
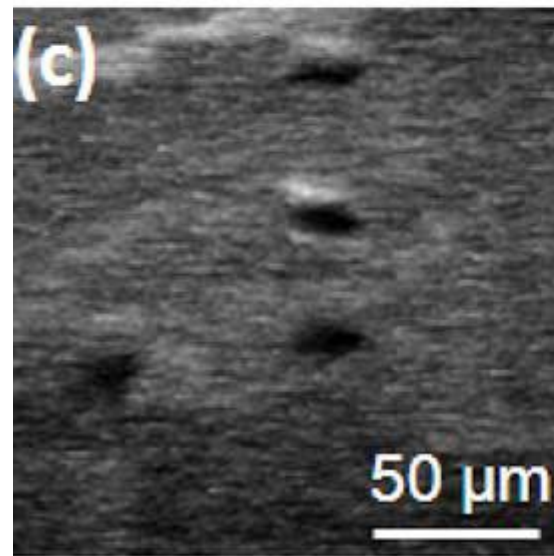
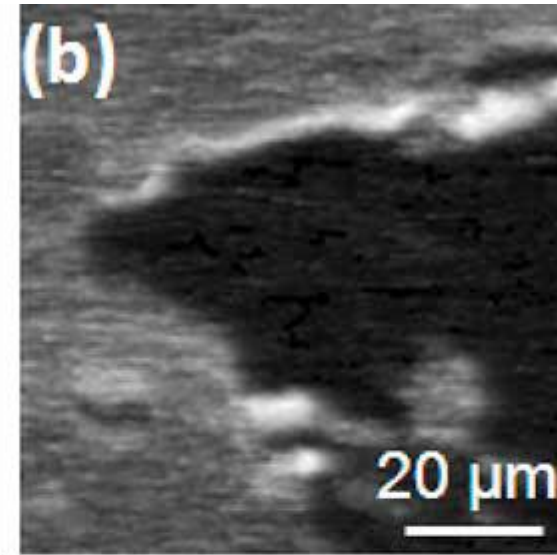
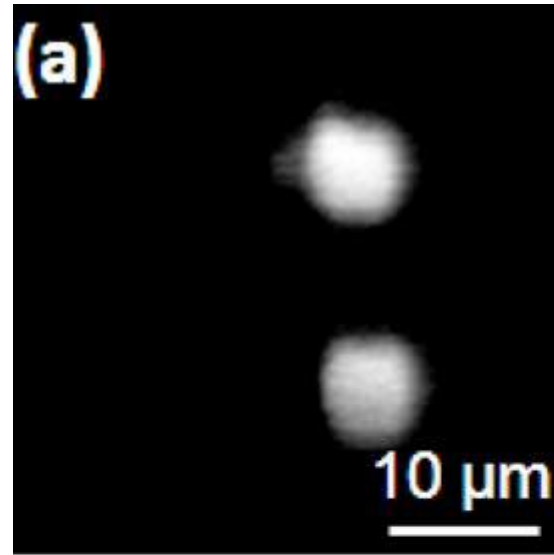
Sample :

(a) 6 μ m beads;

(b) bone structure

(c) and (d) chondrocytes;

(e) white light microscope
photo showing the bovine knee
joint cartilage sample.



summary

Compares the three types of performance of the fiber, it was demonstrated pulses propagating and high collection efficiency ability of DCPCF.

- Compares the three probe design, it was found configuration that provides flexibility for optimum imaging performance and packaging with collimating and focusing lens.

③“Fibroblast contractility and actin organization are stimulated by microtubule inhibitors”

Introduction

The locomotion of fibroblasts and other tissue cells results from their exertion of contractile 'traction' forces on objects and materials

⇒ These cells traction are known to be produced by a cytoplasmic actin(SF : stress fiber) and myosin network

Several lines of evidence have implicated **microtubules** as playing some controlling role in the motility of tissue cells ;

microtubule-depolymerizing drugs : cause regression of growth

⇒ In cancer cells, to act as an anti-cancer agent

In this study...

performed to clarify whether the microtubules to determine what role by exerting traction.

method:

▪ *C3H/10T1/2 mouse embryo fibroblasts*

Eagle's MEM with Hanks' salts, supplemented with 10 % fetal calf serum, penicillin, streptomycin, and 7-5mM-Hepes.

Cells were removed from tissue culture flasks by a brief treatment with trypsin-EDTA solution, and plated onto either glass coverslips or silicone rubber substrata. Cells were used for experimentation 1-5 days after plating.

Experimental equipment

Time-lapse filming

Kodak Plus-X Reversal film, using a Sage time-lapse apparatus attached (Olympus)

Immunofluorescence

▪ Zeiss 63 X, 1-4 n.a. Planapo objective on a Zeiss IM-35 inverted microscope equipped for epi-fluorescence.

▪ Single-labeling of f-actin and
Double-labelling of actin and tubulin:

Result and Discussion

Tractive force is evaluated by the number and size of wrinkles in the rubber.

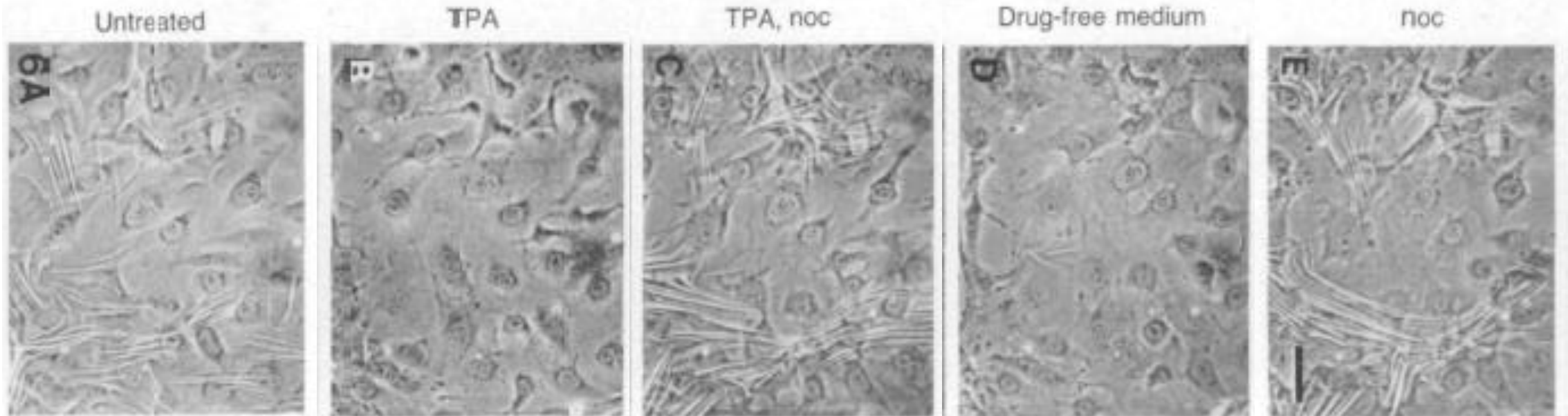
TPA : Tumor marker (But it is normal cell, too)

Noc : Stabilizers

Colcemid

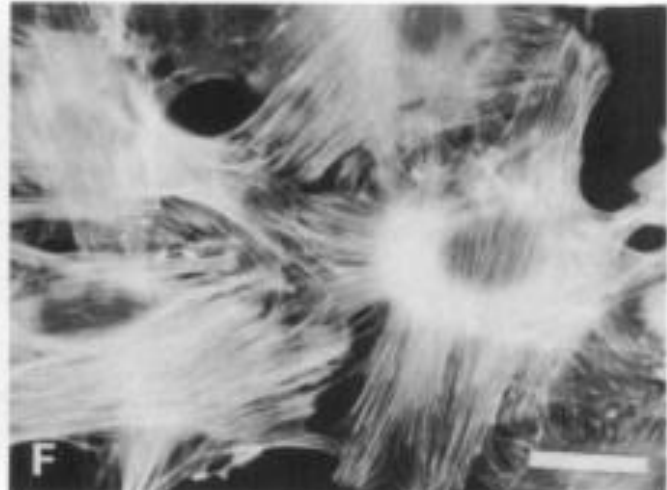
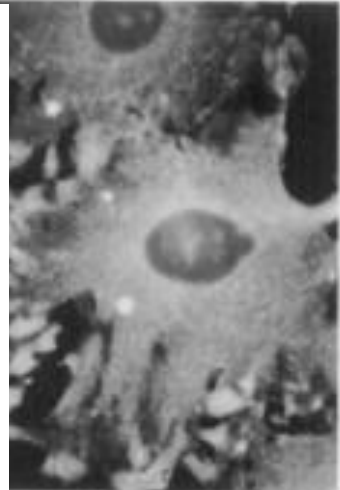
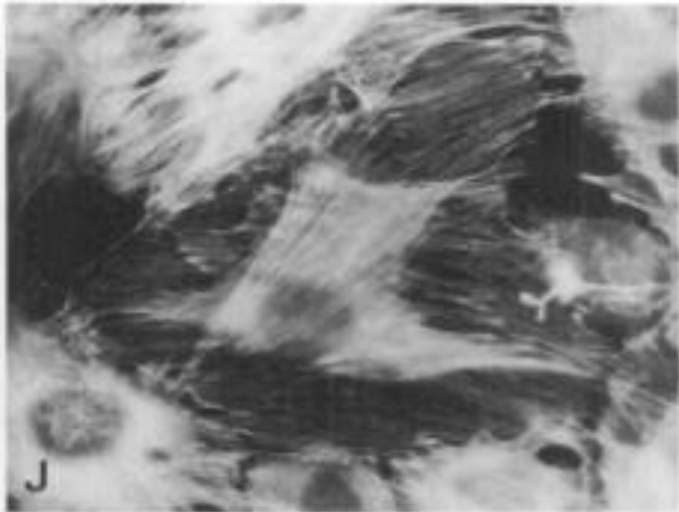
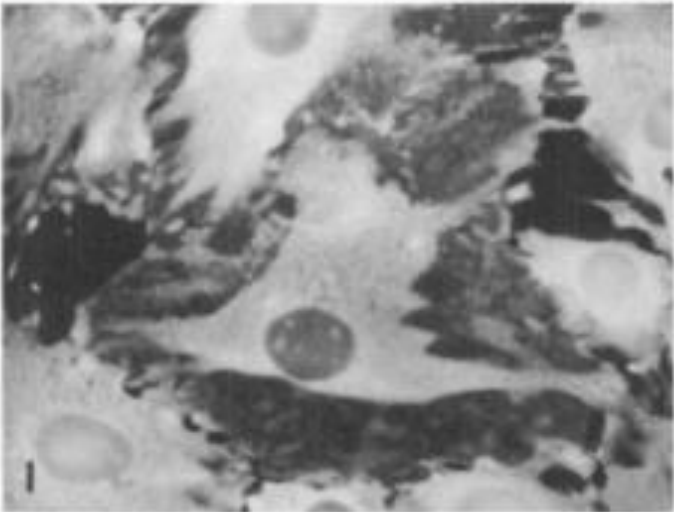
: anticancer drug

VB (vinblastine)



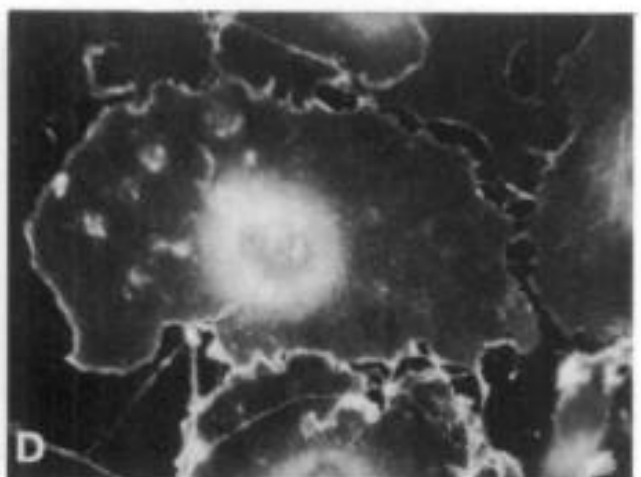
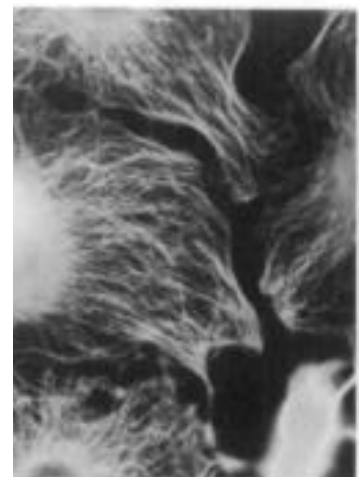
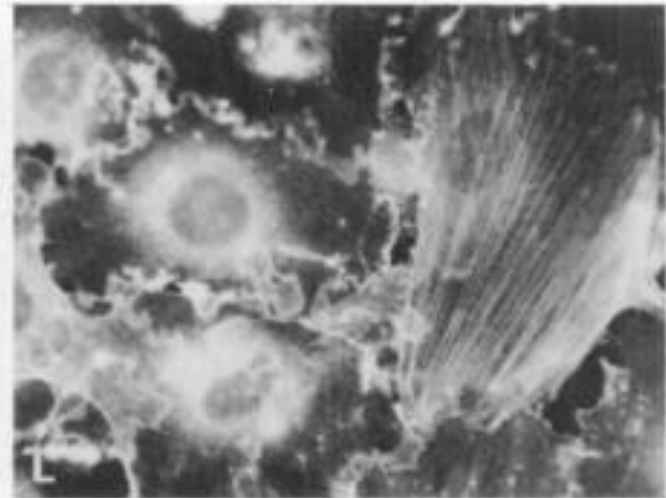
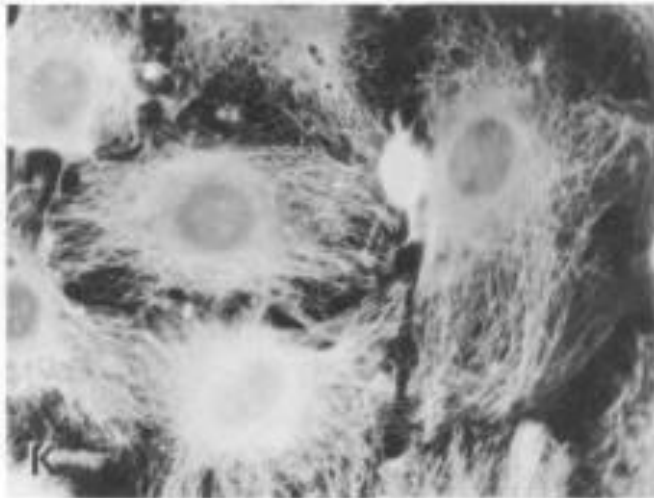
Result and Discussion

TPA, 30 min; noc 60 min



Tublin A C E G I K

1 h after removal of TPA, +noc medium



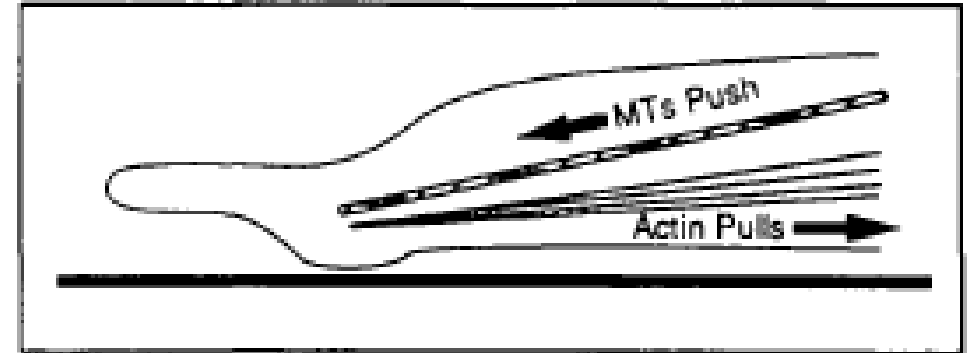
summary

Rather than a gradual change of fibroblasts,
abrupt and change
Recovery of stress fibers was unexpected.

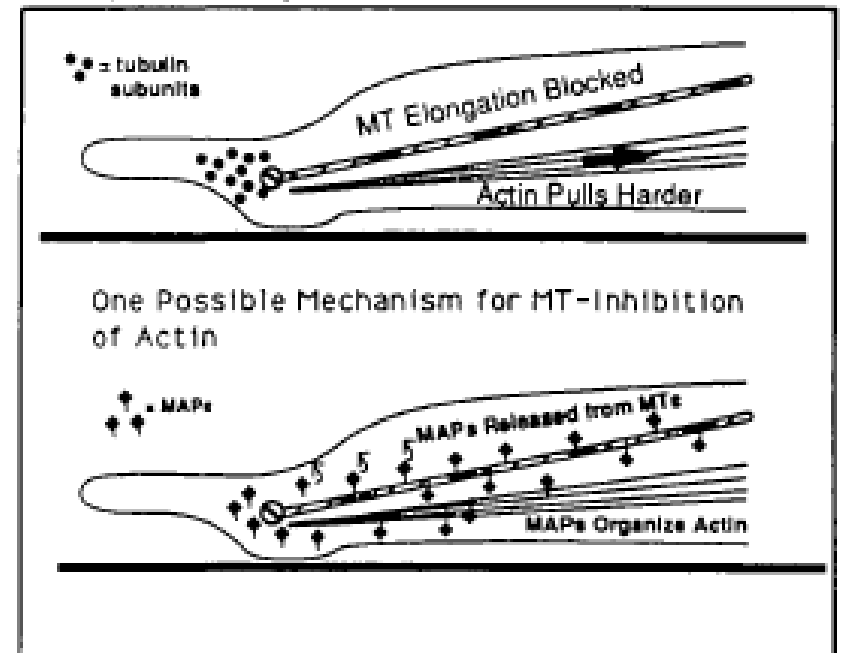
Cytoplasmic Microtubules, it is to exert a large
pressing force, partially offset the pull of actin
stress fibers.

Microtubule-associated protein is secreted, it
interacts with actin SF.

A. Explanation by Tensegrity



B. Explanation by MT-Inhibition of Actin Function



my opinion

- MEMS mirror can be expected wide field of view.
- There is a need for strict design for further miniaturization.
- Old study of fibroblast cells was determined by appearance
⇒ Quantitative evaluation is necessary

That's all.